ABSTRACT

Aim: This study was designed to evaluate the effect of incorporation of hydroxyapatite nanorods into a resin composite restorative material and dental adhesive on shear bond strength to dentin and interfacial micromorphology after storage in different media. Materials and Methods: Ninety natural premolars (N=90) were selected for this study and randomly divided into three main groups (n =30) according to the material used (A), where A1: the resin composite restorative material reinforced with hydroxyapatite nanorods. A2: Adhesive resin material with incorporated hydroxyapatite nanorods, while A3: Resin composite (without nano-hydroxyapatite) as control group. Each group was subdivided into three subgroups (n=10) according the storage media (B) either Acid (B1), artificial saliva (B2) or distilled Water (B3). All specimens were thermocycled then stored at room temperature and kept under each of the above mentioned media for 3 hours every day over 30 days (one month). All samples were individually and horizontally mounted on a Universal testing machine loaded to failure at cross head speed of 0.5 mm/ min then Shear bond strength was calculated. The fractured specimens were tested under scanning electron microscope to examine the dentin adhesive interface and mode of failure. Data were analyzed using one-way analysis of variance (ANOVA) and Tukey’s post hoc significance difference tests. Differences were considered significant at P<0.05. Results: There was a statistically significant difference between groups (p ≤0.05). Adhesive resin with incorporated hydroxyapatite nanorods recorded statistically significant mean higher shear bond strength (6.33±1.53, 11.35±0.78 and 7.97±0.57) after storage in (acid, artificial saliva, distilled water), followed by resin composite incorporates nanorods.

KEYWORDS

Resin Composite,
Hydroxyapatite,
shear bond strength.
(4.86±1.03, 9.31±1.15 and 6.85±0.95) and the least values were for control group (3.11±1.02, 7.3±1.55 and 6.004±1.09). Tukey’s post hoc test revealed a significant difference between each two subgroups. **Conclusions:** Incorporating hydroxyapatite nanorods into the resin composite and adhesive resin greatly improves the shear bond strength to dentin after storage in different media regardless the type of the media and micromorphological observations correlates with the shear bond strength and failure mode.

**INTRODUCTION**

In the era of esthetic dentistry, resin based composites are the material of choice for most restorative procedures. Despite significant improvements, these materials still exhibit deficiencies that impair their longevity. Secondary caries and fracture have been reported as the main reasons for long term failure. Insufficient mechanical strength in load-bearing areas of posterior teeth, high polymerization shrinkage and shrinkage stress remain the key short-comings of resin based composites (1-3).

Several efforts have been proposed to improve the mechanical and biological properties through improvements in the filler packing, optimizing of filler content, development of hybrid fillers. One of these fillers is hydroxyapatite which has been proposed as a filler for composite materials and was later introduced into adhesives at nanometer scale improving several of the material properties (4,5). With development of nanotechnology, a major impact on the material science has been noted. In this century, the production of materials with nanostructures has gained much attention for adsorption, catalytic, biomaterials and optical applications. Hydroxyapatite is the main biomineral found in the human hard tissues (Ca_{10}(PO_{4})_{6}(OH)). It is comprised of calcium and phosphorus present in the ratio (Ca/ P) of 1.67 (6). Hydroxyapatite has attracted much interest as a biomaterial for use in prosthetic applications due to its similarity in crystallography and chemical composition to that of human hard tissue. On account of its outstanding properties like biocompatibility, bioactivity, osteoconductivity, non-toxicity and non-inflammatory nature which have a variety of applications that include bone tissue engineering, endodontic treatment, edentulous ridge augmentation, desensitizing agent post bleaching, treating early carious lesions, fillers for reinforcing restorative glass ionomer cement and restorative composite resin (7). Addition of hydroxyapatite as a filler particle to resin composite was first reported in 1988 by Okazaki and Ohmae which results in improvement of mechanical properties and biocompatibility only when the apetite to resin ratio was maintained at 1 (8). Then later hydroxyapatite nanoparticles have been used in the formulation of restorative composite systems (9,10). Moreover, they were used in dental adhesives to fortify the adhesive bond strength of adhesive to dentin (5). Therefore, the present study aimed at evaluating the effect of incorporation of nano rod hydroxyapatite into a resin composite restorative material and a dental adhesive on shear bond strength to dentin after storage in different media (acid, artificial saliva and distilled water). Furthermore, interfacial micromorphology was also studied.

**MATERIALS AND METHODS**

**Preparation of samples:**

Non- carious ninety natural premolars in persons under the age of twenty- one years were collected, cleaned, scrubbed and scaled to remove blood, mucous, shreds of periodontal ligaments and calculus then stored refrigerated at 4° C in distilled water. The ninety teeth were divided into three main groups of 30 each (n =30) according to the materials used (A), where A1: the resin composite restorative material reinforced with hydroxyapatite nanorods was applied over the bonded surfaces. A2: Adhesive resin material with incorporated hydroxyapatite nanorods was used over dentin surfaces, while A3: Composite resin restorative material (without nano-hydroxyapatite) was used over the bonded dentin surfaces as control group. Each group was further subdivided into three subgroups of 10 each (n=10) according the storage media (B) either Acid (B1), artificial saliva (B2) or distilled water (B3).
Each tooth was embedded in self-cured acrylic resin block which was fabricated by using a plastic mold with dimensions of 1.6 cm diameter and 2 cm height on to which chemically activated acrylic resin (Acrostone, Manufacturing and Import Co., Egypt) was packed. The long axis of the teeth was adjusted parallel to that of the plastic ring using parallometer (AF30, Nouvag, Switzerland). Occlusal surfaces were made flat with double-faced diamond disc by cutting the occlusal surface through a mark made about 3 mm apical to the cusp tips under water cooling until a clean dentinal surface was exposed. The prepared dentin surfaces were then be polished with 180, 320, 600 grit wet silicon carbide paper to stimulate the production of smear layer. All the prepared specimens were then stored for 24 hours in incubator at 37°C.

**Bonding Procedures:**

The prepared dentin surface was etched using 37% phosphoric acid gel for 15 seconds then thoroughly rinsed with water for 15 seconds and excess water was gently blotted dry with the help of cotton pellets. For group (A1, A3) the bonding procedures were done following the manufacture’s instructions by applying two coats of Tetric N-bond (Ivoclar Viva dent) by the help of a fully saturated disposable brush tip, gently dried for 2-5 seconds with air blast and light cured for 10 seconds each using LED unit (Cordless LED curing light system, TPC Advanced Technology, city of industry 91748 USA). For group (A2) the modified adhesive (Tetric-N bond) was shaken well, 2 consecutive coats of the adhesive were applied for 20 seconds with gentle agitation using a brush, gently air thinned with air for 5 seconds to evaporate solvents and light cured for 20 seconds.

**Resin Composite build up:**

For group (A1) Te-Econom Plus resin composite (Ivoclar, Viva dent shade A1) incorporates hydroxyapatite nanorods and for groups (A2, A3) Te-Econom plus resin composite without hydroxyapatite nanorods was dispensed and packed in one increment (bulk packing) using a plastic instrument (Noredent Basic Composite Kit, Norden, Germany) on the dentin surface held in position by the split Teflon mold of dimensions (4 mm in diameter × 2 mm in thickness) then plastic matrix strip (Greko Grgo, Kostunov, 69124, Germany) was placed over the resin composite and gently pressed flat with a glass slab and the excess resin composite was removed by a sharp instrument. After removal of the glass slab, the resin composite was light cured for 20 seconds using LED curing device then the Teflon mold was removed.

**Thermocycling:**

All specimens were subjected to thermocycling procedures in thermocycling apparatus (ROBOTA automated thermo-cycle; BILGE, Turkey) the number of cycles used were 500 cycles and dwell time was 25 seconds in each water bath with a lag time 10 seconds. The low-temperature point was 5°C and the high-temperature point was 55°C corresponding to 6 months clinical use.

**Storage:**

All specimens were stored in different storage media for one month. These media include acid 0.01 M Lactic acid buffer solution of pH4, artificial saliva (pH value 6.75 ± 0.15) and distilled water (Pure water H2O of neutral pH).

**Shear bond strength test:**

After all groups were stored for one month, the specimens were removed from the test solutions and thoroughly cleaned, dried and then subjected to shear bond test which was done using Universal testing machine at cross head speed of 0.5 mm/ min.

**Scanning electron microscope testing:**

The fractured specimens were tested under Scanning Electron Microscope to examine the dentin adhesive interface and mode of failure using Quanta 250 FEG (Field emission Gun) attached with EDX unit (Energy Dispersive X-ray analysis with accelerating voltage 30kv).
Statistical Analysis:

Values of shear bond strength were presented as mean and standard deviation (SD) values. (One way analysis of variance ANOVA test) was used to compare between groups and sub-groups. Two ways analysis of variance ANOVA test was used to study the statistical significance of the interaction between variables (material used and storage medium).

RESULTS

I- Hydroxyapatite nanoparticles characterization results:

The resultant Transmission Electron Microscope (TEM) micrographs showed that the prepared hydroxyapatite nanorods had size ranging between 20-100 nm in diameter and 10-20 nm in length with slight tendency to agglomerate. Photomicrographs of the modified adhesive system and resin composite confirmed the uniform distribution of the nanorods with tendency to aggregate.

II- Shear bond strength results:

There was a statistically significant difference between groups (p ≤0.05). On using acids as storage medium, the greatest mean shear bond strength (6.33±1.53) was recorded for (group A2) followed by (group A1) (4.86±1.03), and the least value was for control group (3.11±1.02). On using artificial saliva as storage medium, the greatest mean shear bond strength (11.35±0.78) was recorded for (group A2), followed by (group A1) (9.31±1.15), and the least value was for control group (7.3±1.55). Tukey’s post hoc test revealed a significant difference between each two groups and finally on using distilled water as a storage medium the greatest mean shear bond strength (7.97±0.57) was recorded for (group A2), followed by (group A1) (6.85±0.95), and the least value was for control group (6.004±1.09). Tukey’s post hoc test revealed no significant difference between group A1 and A3 (control). Two ways ANOVA test was used to test interaction between variables and revealed a significant difference between materials used (rows) (p<0.05), as well as a significant difference between storage media (columns), (P<0.05). However, the interaction between both variables (material used and storage media) was not statistically significant (p>0.05). Values are presented numerically in table (1).

<table>
<thead>
<tr>
<th>Shear Bond Strength (MPa)</th>
<th>B1 (acids)</th>
<th>B2 (artificial saliva)</th>
<th>B3 (Distilled water)</th>
<th>(material used)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td></td>
<td></td>
<td></td>
<td>F</td>
</tr>
<tr>
<td>Group A1</td>
<td>Mean</td>
<td>4.86a</td>
<td>9.31ab</td>
<td>6.84ab</td>
</tr>
<tr>
<td></td>
<td>SD</td>
<td>1.03</td>
<td>1.15</td>
<td>0.95</td>
</tr>
<tr>
<td>Group A2</td>
<td>Mean</td>
<td>6.33aA</td>
<td>11.35Aa</td>
<td>7.97Aa</td>
</tr>
<tr>
<td></td>
<td>SD</td>
<td>1.53</td>
<td>0.78</td>
<td>0.57</td>
</tr>
<tr>
<td>Group A3</td>
<td>Mean</td>
<td>3.11cC</td>
<td>7.3cC</td>
<td>6.004cB</td>
</tr>
<tr>
<td></td>
<td>SD</td>
<td>1.02</td>
<td>1.55</td>
<td>1.09</td>
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<tr>
<td>(storage media)</td>
<td>F</td>
<td></td>
<td></td>
<td>125.09</td>
</tr>
<tr>
<td></td>
<td>P value</td>
<td></td>
<td></td>
<td>&lt;0.0001*</td>
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<tr>
<td>Interaction between variables</td>
<td>F</td>
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</tr>
<tr>
<td></td>
<td>P value</td>
<td></td>
<td></td>
<td>0.0687n</td>
</tr>
</tbody>
</table>

*significant, ns= non-significant at p<0.05

Mean values with different small letters are significantly different within the same row.

Mean values with different capital letters are significantly different within the same column.
III- Failure mode results:

After shear bond strength test, all the failed specimens were examined using USB digital microscope at 50X magnification to determine the nature of their fracture. Failure type was noted as adhesive, cohesive in resin composite, cohesive in dentin or mixed.

Evaluation of failure modes after shear testing indicated that high bond strength groups showed mixed or cohesive modes, while low bond strength groups tended to exhibit adhesive failure mode. Statistical analysis was performed by using Chi square test to study effect of different materials within each storage media on failure mode numerical values are presented numerically table (2).

<table>
<thead>
<tr>
<th></th>
<th>Adhesive</th>
<th>Mixed</th>
<th>Cohesive in dentine</th>
<th>Cohesive in resin composite</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>no %</td>
<td>No %</td>
<td>no %</td>
<td>no %</td>
</tr>
<tr>
<td>A1B1</td>
<td>6 60</td>
<td>2 20</td>
<td>1 10</td>
<td>1 10</td>
</tr>
<tr>
<td>A1B2</td>
<td>2 20</td>
<td>6 60</td>
<td>0 0</td>
<td>2 20</td>
</tr>
<tr>
<td>A1B3</td>
<td>2 20</td>
<td>5 50</td>
<td>1 10</td>
<td>2 20</td>
</tr>
</tbody>
</table>

Chi square in group A1

\[ X^2 = 6.6, \ p=0.359^{ns} \]

<table>
<thead>
<tr>
<th></th>
<th>Adhesive</th>
<th>Mixed</th>
<th>Cohesive in dentine</th>
<th>Cohesive in resin composite</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>no %</td>
<td>No %</td>
<td>no %</td>
<td>no %</td>
</tr>
<tr>
<td>A2B1</td>
<td>3 30</td>
<td>4 40</td>
<td>0 0</td>
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<td>6 60</td>
<td>1 10</td>
<td>1 10</td>
</tr>
<tr>
<td>A2B3</td>
<td>2 20</td>
<td>5 50</td>
<td>1 10</td>
<td>2 20</td>
</tr>
</tbody>
</table>

Chi square in group A2

\[ X^2 = 2.686, \ p=0.847^{ns} \]

<table>
<thead>
<tr>
<th></th>
<th>Adhesive</th>
<th>Mixed</th>
<th>Cohesive in dentine</th>
<th>Cohesive in resin composite</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>no %</td>
<td>No %</td>
<td>no %</td>
<td>no %</td>
</tr>
<tr>
<td>A3B1</td>
<td>5 50</td>
<td>3 30</td>
<td>0 0</td>
<td>2 20</td>
</tr>
<tr>
<td>A3B2</td>
<td>3 30</td>
<td>5 50</td>
<td>0 0</td>
<td>2 20</td>
</tr>
<tr>
<td>A3B3</td>
<td>2 20</td>
<td>4 40</td>
<td>0 0</td>
<td>4 40</td>
</tr>
</tbody>
</table>

Chi square in group A3

\[ X^2 = 2.9, \ p=0.821^{ns} \]

Chi square in all groups

\[ X^2 = 17.463, \ p=0.828^{ns} \]

DISCUSSION

The clinical performance of composite restorations depends in part upon complete adhesion of the restorative composites to enamel and dentin. For enamel, the acid-etch procedure is usually successfully used (11,12) Moreover, oral cavity is a complex environment, where the restorative material is in contact with saliva which contains a variety of inorganic and organic species together with bacterial flora (13). Furthermore, PH changes and thermal cycling from changes in oral temperature provide conditions for degraded bond strength in an aqueous environment (14).

Recently, nanoparticles as hydroxyapatite have been used in the formulation of restorative composite systems with the aim of improving physical and mechanical properties, bioactivity and bond strength of these resin composites to dental structures and have also been incorporated into the dental adhesives (5). The present study was designed to evaluate the effect of incorporation of hydroxyapatite nanorods into a resin composite.
restorative material and a dental adhesive on shear bond strength to dentin after storage in different media (acid, artificial saliva and distilled water).

The results obtained in this study showed that shear bond strength mean values of (Resin composite incorporates hydroxyapatite nanorods) showed a higher statistically significant difference compared to (Resin composite without HA nano rods) when stored in lactic acid (B1) and artificial saliva (B2). This could be attributed to the incorporation of HA nano rods into the resin composite which increased the filler loading that reduces the polymerization shrinkage, water sorption of the resins, thermal expansion coefficient and improve the mechanical strength properties which may in turn improve the bond strength to dentin (15,16).

The increase in the mixed mode of failure at the resin / adhesive interface within resin composite incorporates HA nanorods group (A1) may indicate the strengthening effect and improvement of bond strength. This is in agreement with many studies (17-19). Moreover, these findings are supported by SEM photomicrograph observations which showed thick well formed hybrid layer with numerous resin tags extending into the widely opened dentinal tubules while SEM photomicrographs of group (A3) showed a thin non homogenous hybrid layer and few, weak and faint resin tags extending into the widely opened dentinal tubules and adhesive mode of failure.

Regarding the shear bond strength mean values of adhesive resin incorporates HA nanorods showed the highest statistically significant difference compared to resin composite incorporates HA nanorods) and control group after storage in acid (B1), artificial saliva (B2) and distilled water (B3). This could be attributed to addition of fillers into the adhesive resin that resulted in increase adhesion to the tooth substrate and decrease degradation of the material over time (20, 21). Also, HA fillers may improve adhesive mechanical properties by strengthening the adhesive layer; prevent thinning of adhesive layer providing better relief of composite contraction stresses (22). HA fillers have been shown to increase polymerization rate and degree of conversion thus diminishing polymerization shrinkage and increasing the modulus of elasticity of the adhesive layer which may results in increasing bond strength to enamel and dentin (23). This result was in agreement with many studies (5,24,25).

The shear bond strength results of different subgroups were obviously related to the storage media used in each subgroup. Within resin composite with HA nanorods, Adhesive resin incorporates HA and control group, subgroups stored in lactic acid (B1) had the lowest (SBS) mean and SD values and showed a significant difference compared to those stored in artificial saliva (B2) and distilled water (B3) This could be attributed to detrimental effects of acid on the resin based composites; the fillers tend to fall out from the resin material (26), matrix components decomposed when exposed to low PH environment (27) and the resin based composites were found to undergo greater micromorphological damage. In oral environment, the effect of acids and other solvents may have detrimental and sustained effect on the mechanical properties of resin composites (28).

As for the shear bond strength mean values of subgroups stored in artificial saliva (B2) within group A1 and group A2 showed a high significant difference compared to those stored in lactic acid (B1) and distilled water (B3). This could be attributed to the fact that the artificial saliva contains many minerals like Ca++, PO₄⁻, Na+ and urea during storage, deposition of these minerals on the surface of the resin composite resulted in the formation of film probably composed of calcium on the surface of resin composite increasing the mechanical properties of resin composite (29). The results were in agreement with (30,31) who measured the micro hardness of the resin composite after conditioning in saliva and orange juice and the results showed that the micro hardness increased after storage in artificial saliva.
The shear bond strength mean values of subgroups stored in distilled water (B3) within group A1, group A2 and control group showed a higher significant difference compared to those stored in lactic acid (B1) but in the same time showing a lower shear bond strength values than those stored in artificial saliva (B2). This could be attributed to the fact that on immersion of resin composite in water two processes took place; first, swelling of the resin composite and second, leakage of unreacted monomers and dissolution of resin composite owing to hydrolytic degradation \(^{(18)}\). The results were in agreement with \(^{(32,33,34)}\) who suggested that water sorption into the demineralized dentin might cause hydrolytic degradation of the collagen fibrils at this zone leading to decrease in bond strength.

**CONCLUSIONS**

Within the limitations of this study, the following could be concluded:

1. Incontrporating 1wt% Hydroxyapatiten norods into the resin composite (Te-Econom Plus) had greatly improved the shear bond strength to dentin after storage in different media regardless the type of the media used in the study.

2. Modifying the adhesive system (Tetric –N bond) by 2wt% hydroxyapatite nanorods provided a superior improvement in shear bond strength of the resin composite to dentin and produced adhesive system that is less prone to degradation.

3. Micromorphological observations at the interface between resin composite and dentin correlates with the shear bond strength and the failure mode.

**REFERENCES**


